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# Formulation & Characterization of Sustained Release: Multichambered Tablet of Losartan Potassium Using Fused Deposition Modelling (FDM) 3D-Printer

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|---|--|---|--|--|--|
| <b>KEYWORDS</b><br>3D-Printing, Fused<br>Deposition<br>Modelling, Sustained<br>Release, Additive  | <b>ABSTRACT:</b><br><b>Introduction</b> : The Aim of present research work was to formulate and characterize Sustained release: Multichambered Tablet Using Fused Deposition Modelling (FDM) 3D-Printer, the drug candidate used in this project was Losartan Potassium, is an Angiotensin receptor Type -II blocker.  |   |  |  |  |
| Manufacturing, Poly<br>vinyl Alcohol  | <b>Objectives</b> : By alte tablet using API Lo  | ring the shell thickness and infill sartan Potassium had been achiev  | density %, sustained release action of ved.  |  |  |
| (PVA), Rapid<br>prototyping Methods: The<br>Method". Tabl<br>and FIII) by cr<br>1.5 mm respect<br>1.5–2hrs (Indi<br>enhanced the<br>extended upto | Methods: The Now<br>Method". Tablets w<br>and FIII) by creatin<br>1.5 mm respectively<br>1.5–2hrs (Indian Ph<br>enhanced the bioav<br>extended upto 270m   | rel method had been used for fab<br>vas prepared using FDM 3D-print<br>g variation in infill-density and in<br>y using poly vinyl alcohol (PVA<br>harmacopoeia, 2018) with poor b<br>ailability of the drug, the <i>in-vitra</i><br>nins (approx.). | pricating Tablet called "Pause and fill<br>er with three different batches (FI, FII<br>nner wall thickness: $0.5$ mm, 1mm and<br>a) filament. As half-life of Losartan is<br>ioavailability, sustained release tablet<br><i>o</i> drug release from the tablet drug is |  |  |
|   | <b>Results</b> : From the I<br>with drug release a<br>and FI shows 97.7<br>states that the coeff<br>by zero order release  | Results it concluded that the FIII<br>bout 99.23 % for 270 mins, whe<br>1% for 210 mins. The data wher<br>icient 'r' indicated the drug releas<br>se kinetics.  | batch of tablet is the optimized batch<br>reas FII shows 98.69 % for 240 mins<br>a used to evaluate the kinetic studies,<br>se from the tablet which was followed  |  |  |
|   | <b>Conclusions</b> : The producing rapid and also helps to decreat increase the safety a release characteristic devices with different devices with devices with different devices with different devices with | work conclude that the FDM and a sustained release tablets on the lase the side effects of drugs by p and efficacy and avoid incompations. The printer software enabled ent wall or chamber thickness.  | 3D printing process was capable for<br>basis of different thickness. This work<br>roviding sustained release of drugs &<br>ble between APIs by developing drug<br>easy fabrication of oral drug delivery   |  |  |

### 1. Introduction

Novel Drug delivery systems are the techniques which are day by day getting more developed and more accurate for delivering of therapeutic doses, which are tailored according to the patient need or requirement. Additive manufacturing technology includes various types of 3Dprinting methods are as follows: Stereolithography (SLA), selective laser sintering (SLS), inkjet-based 3D- printing and Fused deposition modelling (FDM). Such novel methods can be used in choosing the doses i.e, flexibility in selection of amount of drug or API, shape and size of the dosage, etc<sup>1–3</sup> A Rapid proto-typing technology, due to it's cheapest printing costs, high printing quality, and well capacity to employ drug-loaded filaments via hot-melt extrusion (HME), Fused deposition modelling (FDM) is one of the additive

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manufacturing techniques that is most oftenly researched or used for formulating dosage forms, or even in case of bioprinting in medical emergencies <sup>4,5</sup>.

The "three Ds of 3D printing" refers to the overall procedure of 3D-printing method. These are (i) Design, (ii) Development and (iii) Dispense. This technique is only now beginning to be adopted by the pharmaceutical sector. There aren't any significant companies in the pharmaceutical sector creating drugs for regular use. Chuck Hull's stereolithography apparatus (SLA) received the first patent in 1986, which is when 3D printing initially emerged. He is regarded as the originator of 3D printing technology as well printing in the biomedical and pharmaceutical industries or field had been introduced in the year of 2015 <sup>6–8</sup>. Numerous firms are investigating this possibility, including Teva and Aprecia Pharmaceuticals. A high medication load, up to 1,000 mg, may be delivered in a single dosage thanks to ZipDose Technology. By administering even the highest concentrations of levetiracetam with only a sip of drink, "SPRITAM" was authorized by the US Food and Drug Administration (FDA) on year August 3, 2015, to treat partial-onset, myoclonic, and generalized tonic-clonic seizures improves the patient experience. Using 3DP technology, which was developed at Massachusetts Institute of Technology, Aprecia created its ZipDose Technology platform 9-11

An appropriate polymer is chosen, melted, and then pushed or introduced through a heated nozzle out that may be moved. The polymer is applied layer by layer along all three following axis i.e, (x, y, and z axis), and when it get solidified, it takes on the precise shape as per the computer-aided design (CAD) models had intended into machine <sup>12–14</sup>. The invention and experiments using 3D -printing method had been described illustratively in **Figure 1** 



Figure 1: Inventions & Experiments using 3D-Printing

### 2. Objectives

The aim of this research work is that the FDM 3D printing process was capable for producing rapid and sustained release tablets on the basis of different thickness. This work also helps to decrease the side effects of drugs by providing sustained release of drugs & increase the safety and efficacy and avoid incompatible between APIs by developing drug release characteristics. The printer software enabled easy fabrication of oral drug delivery devices with different wall or chamber thickness. DSC and HPLC are carried to check the identification and purity of drug. All results are within the acceptance range. DSC data showed that the Losartan Potassium drug was unaffected by the printing and that there were no detectable interactions. PVA compartments are designed by the use of CAD software (Auto-CAD) in two steps. First printing of the tablet upto 75% and then paused, again after the API filling manually the rest part of the body building up. PVA reservoir were fabricated in three different batches on the basis of different thickness of inner most walls and difference in infill densities (FI, FII, FIII).

The 3D printed tablets were evaluated for Size and shape, hardness, weight variation, dye test and drug release test. All results are within acceptable range as defined by Indian Pharmacopoeia. In drug release performance we found the best result from FIII batch because it showed up for longest period of time amongst the three batches of formulation i.e, sustained release action upto 270 mins (approx.) In this system the drug resent in the outer compartment or chamber with thin wall is released first and release of the drug in the thick layer of compartment only commences when the thin lay er is practically dissolved. Drug release kinetic data of the 3D printed (FIII) batch of tablet analyzed and found to be fitted into zero order drug release kinetics. First order, Higuchi and korsmeyer-peppas model. Almost all formulations were well fitted in zero-order drug release kinetics with the highest linearity

#### 3. Methods

#### Model Designing of 3D- Tablet

The tablet model had been designed using CAD software (Auto-CAD), then the STL file is further sliced using Cura-Ultimaker and converted into G-code format file i.e, Machine readable format. The filament which was used

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for the fabrication of the sustained release multichambered tablets namely Poly-vinyl Alcohol (PVA) filament. PVA is a water- soluble, biodegradable Polymer which is widely used by the researchers in the preparation or fabrication of the Pharmaceutical Formulation using 3D- Printer, due to its flexibility and physiochemical properties. **Figure 2** provides brief working of 3D- printing process<sup>15</sup>.

This section outlines plan and how the process had been carried out. In this study "Pause and fill method". The structure was printed by a single-nozzled (0.4 mm in diameter) FDM 3D printer (3D-Prototyperz, DEX 200, Indore, India). The filament which is used to fabricate the Tablet is Poly vinyl alcohol (PVA) which is a watersoluble and biodegradable polymer. This Tablet is having 2 hollow chambers in which the drug (API) is to be filled shown in Figure 3 The outer most chamber wall is having thickness of 1.5mm and the inner-most wall thickness is about 1.0 mm. The command had been given to the 3D-Printer using SD card in which the design of the tablet is saved in the format of g-code. The g-code file must be containing the command of stop i.e; after the completion of 75-80 % of the printing of tablet the machine will automatically be paused and then the desired dose will be poured into the different cavities or chambers of the tablet as per the need, then again just "press" print again and the remaining portion of the tablet will be printed successfully.



Figure 2: Flow chart showing processing of 3D-Printing of object

The printer parameter was adjusted by the 3D slicing software namely "Auto-CAD software" are as follows: a layer height of 0.1 mm, printing speed 10 mm/sec., infill density of 40%, 75% and 100% (FI, FII, FIII) respectively. The nozzle temperature were set to be at temperature 210 °C and the bed or printer tray temperature at 60 °C <sup>16,17</sup>.



Figure 3: Printing procession of Tablet (After completion of 75% the nozzle is moved back, for the filling of the API)

#### 4. Results

Losartan Potassium loaded Sustained Release: Multichambered Tablet were prepared successfully using Fused Deposition Modelling 3D- Printing method. The three batches of tablets had been prepared with different infill densities and inner-wall thickness, FI, FII and FIII with 40%, 75% and 100% infill density respectively. And the results were evaluated and observed as follows – **Size, Height, mass, width:** 

The shape of the tablet fabricated was circular containing chambers or cavities in the form of different layers vertically. The Diameter of the tablet was found to be 13 mm and height 0.5 mm. Three batches of the formulation were formulated i.e, FI, FII and FIII with different infill densities are as followed – 40%, 75% and 100% enlisted in **Table no. 1** 

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The thickness and the difference in the infill density of the tablet so the weight of the tablet found to be consequently increasing i.e, FI - 0.11% < FII - 0.27% <FIII - 0.39%. All the tablet batches were passed the weight variation test and within the acceptable limit (less than ±5 %) according to USP weight variation limit.

### Differential scanning calorimeter (DSC)

DSC study was carried out to check the compatibility between Losartan Potassium and PVA filament used in the formulation. It is carried out to confirm that there should be complete physical compatibility of drug and filament with no mutual interaction. DSC thermogram of Losartan Potassium exhibited an endothermic peak at 278 °C followed by **Figure 4** 



Figure 4: DSC report of Losartan Potassium

Whereas, the mixture of drug (Losartan) and polymer (PVA filament) was kept in an accelerated condition of 40 °C/75% RH for 10 days and subjected to DSC analysis. The mixture exhibits endothermic peak which was found approx. 275.34



°C, which suggested clearly that there was no interaction between Losartan Potassium and PVA filament and the drug Losartan Potassium was existed in it's unchanged form **Figure 5** 



Figure 5: DSC report of mixture of PVA and Losartan Potassium

High Performance Liquid Chromatography (HPLC) The chromatographic separation was performed using  $C_{18}$  column (250mm x 4.6mm x 5.0µm) including a Rheodyne injector with 10 µl fixed loop. Empower software had been used for the data analysis and interpretation. The mobile phase consists of 2 solvents: 0.1% Ortho-phosphoric acid (OPA) considered as mobile phase (A) and Acetonitrile (ACN) as, mobile phase (B) in ratios 75:25, 10:90, 75:25, 75:25 followed by I.P, 2018 edition. Run time of the method was set at 55 mins. The flow rate of the sample was 1ml/min. The readings are – *ref.* **Table 2 and Figure 6 & 7** 

Table 2: - HPLC report conc./area

| S. No. | Concentration (ppm) | Area (AUC) |
|--------|---------------------|------------|
| 1.     | 10                  | 413061     |
| 2.     | 20                  | 760424     |
| 3.     | 30                  | 1129993    |

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Figure 6: Graph of Losartan Potassium showing linearity Conc. (ppm)/AUC



Figure 7: HPLC spectrum of Losartan potassium

#### **Hardness Determination**

The hardness measured of the tablet of each batch between 5-6.5 kg/cm<sup>2</sup>. According to Indian pharmacopoeia  $5.5\pm0.06$  and  $7.5\pm0.06$  kg/cm<sup>2</sup> is the hardness limit of the matrix tablet which depicts good mechanical strength of tablet. It was due to the plasticity nature of the PVA. Hardness of the 3D- Printed Tablet is shown in **Table no- 3** 

| <b>Fable 3:</b> - | Hardness | of 3D- | Printed | tablets (1                            | n=3) |
|-------------------|----------|--------|---------|---------------------------------------|------|
|                   |          |        |         | · · · · · · · · · · · · · · · · · · · |      |

| Formulation | Hardness (kg/cm <sup>2</sup> ) |     | /cm <sup>2</sup> ) | Average Hardness<br>(kg/cm <sup>2</sup> ) |
|-------------|--------------------------------|-----|--------------------|---|
| FI          | 5.8                            | 6.2 | 5.9                | 5.9 ±0.61                                 |
| FII         | 6.0                            | 5.5 | 6.2                | 5.9 ±0.13                                 |
| FIII        | 5.5                            | 6.5 | 6.4                | 6.1 ±0.33                                 |

#### Dye Test

The results of Dye test reveals that the methyl orange starts releasing between 30 mins to 120 mins i.e, The outer chamber wall started dissolving between 30-120mins. whereas, inner chambers wall start dissolving and the methylene blue start releasing between 180 mins. to 270 mins. as shown in **Figure 8** 



Figure 8: Photographs of dye test

#### In-vitro Drug release

Dissolution study had been carried out at 0.1 N HCl medium at 205nm by maintaining the temperature about 37 °C  $\pm$  0.5 °C of the medium to mimic human stomach environment for all the three batches of tablet and the results clearly shows that the drug percentage release profile of the batch three i.e, FIII with infill density 100% and inner chamber wall thickness upto 1.5mm is having extended time duration and better drug release profile comparatively to the other two batches (FI and FII) of formulations shown in **Figure 9-**



Figure 9: Percentage Drug release of 3D- Printed Tablet

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### Drug release kinetics mechanism study

The kinetics of *in-vitro* drug release was calculated by applying the data of drug released to various kinetic model such as Zero order, First order, Higuchi and Korsmeyer – peppas. And the result obtained is shown in **Table 4**. From the results of kinetic studies, the coefficient 'r' indicated that the drug release followed zero order release kinetics. It was found that the value of 'r' for zero order ranged from 0.9651 to 0.9902, which is near to 1 when compared to first order ranged from 0.8089 to 0.9123. So, it was understood to be following zero order release pattern followed by all three formulations shown in **Figure 10** and **11**-











(c)

**Figure 10:** Graph between cumulative % drug release v/s time of Losartan Potassium (a) Formulation -I, (b) Formulation – II, (c) Formulation – III

| Table 4: - Kine | tic data of 3D | - printed Tablet |
|-----------------|----------------|------------------|
|-----------------|----------------|------------------|

| Formulation | Zero order (r <sup>2</sup> ) |
|-------------|------------------------------|
| FI (40 %)   | 0.9648                       |
| FII (75%)   | 0.9651                       |
| FIII (100%) | 0.9902                       |





### 5. Discussion

In conventional dosage form drugs, which are Amorphous nature, flocculent and low-density character is difficult to compress into a tablet. Hygroscopic drugs are not suitable for compressed tablets. Some limitations and problems like poor patient compliance, dose variation etc. Conventional dosage form has drawbacks like poor bioavailability and fluctuations in plasma drug level and are unable to achieve sustained release. Conventional oral dosage forms such as tablets or capsules undergo many production steps eg, granulation, compaction, size reduction, tableting or coating. In other hand, 3D printing reduces production to one or two steps, depending if there is pharmaceutical material in filament from available. 3D printing can revolutionize the world. 3D printing used to modify medicines as per the patient requirement involving the potentially to select optimal dose, appearances and release profile. Fused deposition modelling (FDM) is one of the most widely used 3D printing techniques to make solid dosages and offers accurate dosage by adjusting the parameters in CAD.

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This paper aim was to formulate and evaluate 3D printed Sustained Release: Multi-chambered Tablet using Fused Deposition Modelling (FDM) technology. The 3D printer uses a fixed amount of drug and polymer to print which minimizes the dose variation of the drug. Result accurate and precision dosing of the drug to the patients. Keeping in view of the above benefits, our aim was to explore 3D printing technology for formulation suitable dosage form of drug which may lead to reduce the dosing frequency, manufacturing cost and increase the patient compliance.

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